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A general framework for dynamic cortical function: the function-through-biased-oscillations (FBO) hypothesis

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Abstract

A central goal of neuroscience is to determine how the brain's relatively static anatomy can support dynamic cortical function, i.e., cortical function that varies according to task demands. In pursuit of this goal, scientists have produced a large number of experimental results and established influential conceptual frameworks, in particular communication-through-coherence (CTC) and gating-by-inhibition (GBI), but these data and frameworks have not provided a parsimonious view of the principles that underlie cortical function. Here I synthesize these existing experimental results and the CTC and GBI frameworks, and propose the function-through-biased-oscillations (FBO) hypothesis as a model to understand dynamic cortical function. The FBO hypothesis suggests that oscillatory voltage amplitude is the principal measurement that directly reflects cortical excitability, that asymmetries in voltage amplitude explain a range of brain signal phenomena, and that predictive variations in such asymmetric oscillations provide a simple and general model for information routing that can help to explain dynamic cortical function.

1. Introduction

Humans are able to rapidly adapt their behavior based on different task demands. While research over the past decades has shown that the structure of the brain is plastic, such as that shown in rapid changes in dendritic boutons during learning (Moser et al., 1994; Piccioli et al., 2014), the long time scale, typically minutes, for such plastic changes in anatomy cannot readily explain changes in function on the time scale of seconds. In pursuit of the search for potential mechanisms that can support this dynamic nature of the brain, studies have produced a large number of experimental results and two influential conceptual frameworks.

These studies occur at different levels of inquiry that span the microscopic domain (i.e., single-neuron neurophysiology) and the macroscopic domain (e.g., electroencephalography (EEG) or behavioral state). Single-neuron neurophysiology studies often directly relate different physiological

40 processes. For example, many studies showed that cortical neurons preferentially fire during the
41 trough of neuronal oscillations in different frequency bands, such as the theta (4-8 Hz) or alpha (8-12
42 Hz) bands (Bragin et al., 1995, Buzsaki et al., 2004, Fell et al., 2011, Haegens et al., 2011, Harris et
43 al., 2003, Huxter et al., 2003, Jacobs et al., 2007, Klausberger et al., 2004, Lee et al., 2005, Lorincz et
44 al., 2009, Siapas et al., 2005). This demonstrates that oscillatory activity can dynamically modulate
45 the excitability of local neuronal populations, which appears to be important for explaining dynamic
46 brain function.

47 Other microscopic or macroscopic studies cannot or do not make explicit statements about
48 particular physiological processes. Rather, they apply mathematical procedures to particular brain
49 signal measurements and report the observed relationship of the resulting brain signal features with a
50 particular behavioral or other measurement. For example, in numerous studies scientists applied
51 specific mathematical techniques (such as the Hilbert transform) to the (usually bandpass-filtered)
52 time-varying brain signal voltage measurements to calculate time-varying estimates of the power or
53 phase of oscillatory activity in a particular frequency band. An increasing number of reports have
54 shown that such power or phase measurements can be related to cortical excitability (e.g., Sauseng et
55 al., 2009 or Canolty et al., 2006, respectively). The results for oscillatory phase in these studies
56 suggest that cortical processing is more likely to occur during a specific phase (usually the trough) of
57 the underlying oscillations (i.e., phase-amplitude coupling (PAC)). While important problems with
58 present PAC signal analysis approaches and their resulting physiological interpretation have been
59 recognized (Aru et al., 2014), the results of these studies do echo the results of the basic
60 neurophysiology studies described above. At the same time, this seemingly direct link to underlying
61 physiological processes does not exist for (the purely mathematical construct of) oscillatory power.
62 In other words, it is unclear how oscillatory power may mechanistically alter cortical excitability.
63 Furthermore, it is unclear why cortical excitability appears to be related to two mathematically
64 completely independent measurements (power and phase) of oscillatory activity.

65 The relationship of different brain signal features with each other and with cortical excitability is
66 even less clear for other types of brain signal features. For example, for the past several decades,
67 scientists have studied different types of evoked responses (ERPs) such as the P300 (Chapman et al.,
68 1964), or different types of slow task-related activity (Bereitschaftspotential (BP, Kornhuber et al.,
69 1965), contingent negative variation (CNV, Walter et al., 1964), or slow cortical potentials (SCPs;
70 Birbaumer et al., 1990, He et al., 2009)). These electrophysiological signals often receive different
71 names that may depend not only on the filtering technique (e.g., spectral analysis vs. signal
72 averaging), but also on the specific area of study. For example, scientists who study the neural basis
73 of movements may call a slowly developing negative potential preceding movements a
74 Bereitschaftspotential (BP, Kornhuber et al., 1965); scientists who study consciousness may call a
75 similar phenomenon a slow cortical potential (SCP, He et al., 2009); and scientists who study
76 response anticipation may call it contingent negative variation (CNV, Walter et al., 1964). These
77 differing naming conventions persist even though these observations share some apparent similarities
78 (in that they are usually reflected in negative voltage shifts), and even though there are observations
79 that link them to other (e.g., frequency-based) phenomena (He et al., 2009, Shibasaki et al., 1978).
80 Similar comments about naming convention could also be made about the large number of different
81 evoked responses (ERPs) that result from actual or anticipated sensory stimulation (e.g., the P3a and
82 P3b (Polich, 2007)). Finally, recent advances in the local field potential (LFP) and ECoG literature
83 have revealed a number of additional brain signal features that express the relationship between the
84 phases or amplitudes of oscillatory activity at single or across multiple sites (e.g., phase-phase or
85 amplitude-amplitude coupling (Buzsaki et al., 2012, Siegel et al., 2012)). The functional relevance

86 and generating mechanism for these phenomena are currently still largely unclear.

87 Nevertheless, there have been some proposals for mechanisms that could explain different types
88 of brain signal features. For example, scientists have tried to explain the generation of evoked
89 responses by phase resetting (Fell et al., 2004, Hanslmayr et al., 2007, Makeig et al., 2002, Sayers et
90 al., 1974), additions to ongoing oscillations (Makinen et al., 2005, Mazaheri et al., 2006, Shah et al.,
91 2004), or non-zero baselines (Mazaheri et al., 2008, Nikulin et al., 2007).

92 Despite these present difficulties in understanding how the brain may support dynamic function of
93 individual neuronal populations, scientists have proposed two influential conceptual frameworks to
94 begin to explain rapid variations in behavior across neuronal populations. The first proposal is the
95 *communication-through coherence* (CTC) hypothesis put forth by Pascal Fries (Fries, 2005). The
96 CTC hypothesis is concerned with the mechanism by which the brain may modulate the functional
97 relationship between one sending and one receiving neuronal population. Specifically, CTC's
98 principal thesis is that function may emerge from anatomy through the brain's ability to optimize
99 information transfer by synchronizing the timing of oscillatory activity at the sending and receiving
100 sites. This hypothesis rests fundamentally on the physiological concept of variable cortical
101 excitability, i.e., neuronal firing occurs preferentially at the trough of oscillatory activity (Haegens et
102 al., 2011, Klimesch et al., 2007, Lorincz et al., 2009). CTC has received support from modeling
103 studies (Akam et al., 2010, Akam et al., 2012) and experimental results (Roberts et al., 2013,
104 Saalman et al., 2012). In sum, CTC is fundamentally based on oscillatory phase: it explains
105 variable function of a sending and a receiving neuronal population primarily through the degree of
106 phase synchrony of modulatory oscillatory activity at those populations.

107 The second proposal is the *gating-by-inhibition* hypothesis that was formally articulated by Jensen
108 and Mazaheri (Jensen et al., 2010). This hypothesis is based on a long history of research by a
109 number of scientists, including Pfurtscheller, Klimesch, Jensen and others. In contrast to the CTC
110 hypothesis, gating-by-inhibition is fundamentally based on oscillatory power: it suggests that
111 neuronal populations that are not related to the task are functionally inhibited by increased oscillatory
112 power in specific frequency bands, such as the alpha (8-12 Hz) band. How this concept, which is
113 based on oscillatory power, may be related to the CTC hypothesis, which is based on oscillatory
114 phase, is uncertain.

115 In summary, while existing theories have made important progress, our understanding how the
116 microscopic concept of cortical excitability relates to different types of macroscopic brain signal
117 measurements and in turn to organized behavior still appears to be incomplete. Furthermore, it is
118 currently unclear how oscillatory power and phase may interrelate with each other, and if and how
119 the conceptual frameworks proposed by Fries and Jensen can be reconciled. Primarily because of
120 these important issues, different neural or behavioral domains are usually described by independent
121 sets of relatively narrow scientific explanations, which tends to force scientists in a particular
122 discipline to stay within and to conform to the corresponding set of explanations. This situation
123 presents a roadblock to an improved understanding of the function of the brain.

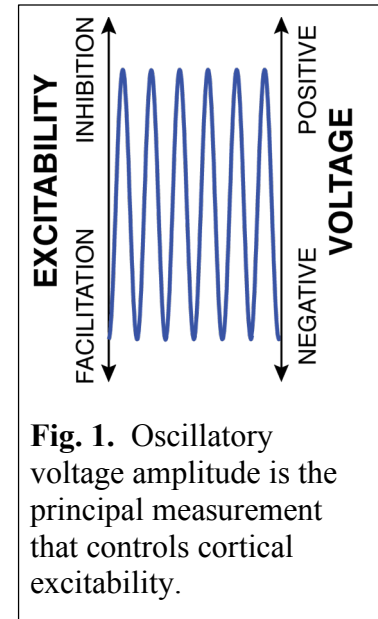
124 Here I provide a conceptual framework of cortical function that may help to resolve these
125 important problems by synthesizing existing experimental results and theoretical models into two
126 general principles. The first principle of this framework suggests that cortical excitability of a
127 neuronal population is indexed most directly by the voltage amplitude of oscillatory activity. This
128 leads to the notion that the established findings of the relationship of oscillatory power or phase with

129 cortical excitability are essentially indirect by-products of asymmetrically distributed peak/trough
 130 amplitudes (i.e., biased oscillations), and that such biased oscillations may underlie a range of other
 131 brain signal phenomena. The second principle embeds biased oscillations in a predictive context,
 132 applies the result to populations of neurons, and thereby reconciles and extends the CTC and gating-
 133 by-inhibition hypotheses. I will refer to the framework that encompasses these two principles as the
 134 function-through-biased-oscillations (FBO) hypothesis throughout this paper.

135 2. The FBO Hypothesis

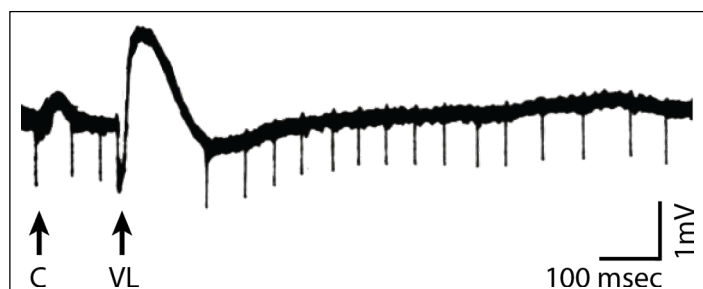
136 2.1. The First Principle: Biased Oscillations Link Cortical Excitability to a Range of Brain 137 Signal Phenomena

138 The first principle of the FBO hypothesis begins with the proposal that
 139 the instantaneous voltage amplitude of oscillations, rather than
 140 oscillatory power or phase, is the principal measurement that directly
 141 reflects cortical excitability. Specifically, I suggest that, for the
 142 exemplary oscillation shown with the blue trace in Fig. 1, the y axis
 143 simultaneously represents cortical excitability as well as oscillatory
 144 voltage. (This exemplary oscillatory activity is shown to be
 145 sinusoidal, but in reality may take on different shapes.)



146 Experimental evidence supports this proposed link between changes in
 147 instantaneous voltage and cortical excitability. For example, Fig. 2
 148 shows recordings from cat motor cortex about 0.2 mm below the
 149 cortical surface. Spontaneous firings of motor action potentials are
 150 clearly visible. Stimulation of the nucleus ventralis lateralis (i.e., the
 151 thalamic nucleus projecting to that area of cortex), but not stimulation
 152 of a nearby cortical site, changes the voltage potential and temporarily
 153 suspends action potential firing. In other words, thalamocortical
 154 volleys appear to shift the cortical voltage
 155 potential away from its baseline¹ so as to
 156 hyperpolarize cortical populations and
 157 thereby inhibit their firing. Similar effects
 158 have been found in the visual cortex (Tasaki
 159 et al., 1954, Von Baumgarten et al., 1952)
 160 and somatosensory cortex (Li et al., 1956).
 161 Thus, rhythmically occurring volleys (such
 162 as those produced by oscillatory activity)
 163 would periodically inhibit a particular
 164 neuronal population in the cortex. This
 165 resulting interpretation of the functional role
 166 of oscillatory activity is consistent with an
 167 emerging view on this topic (Klimesch et al.,
 168 2007, Mathewson et al., 2011).

169 It is important to recognize that, in the
 170 example in Fig. 1 that features a constant and

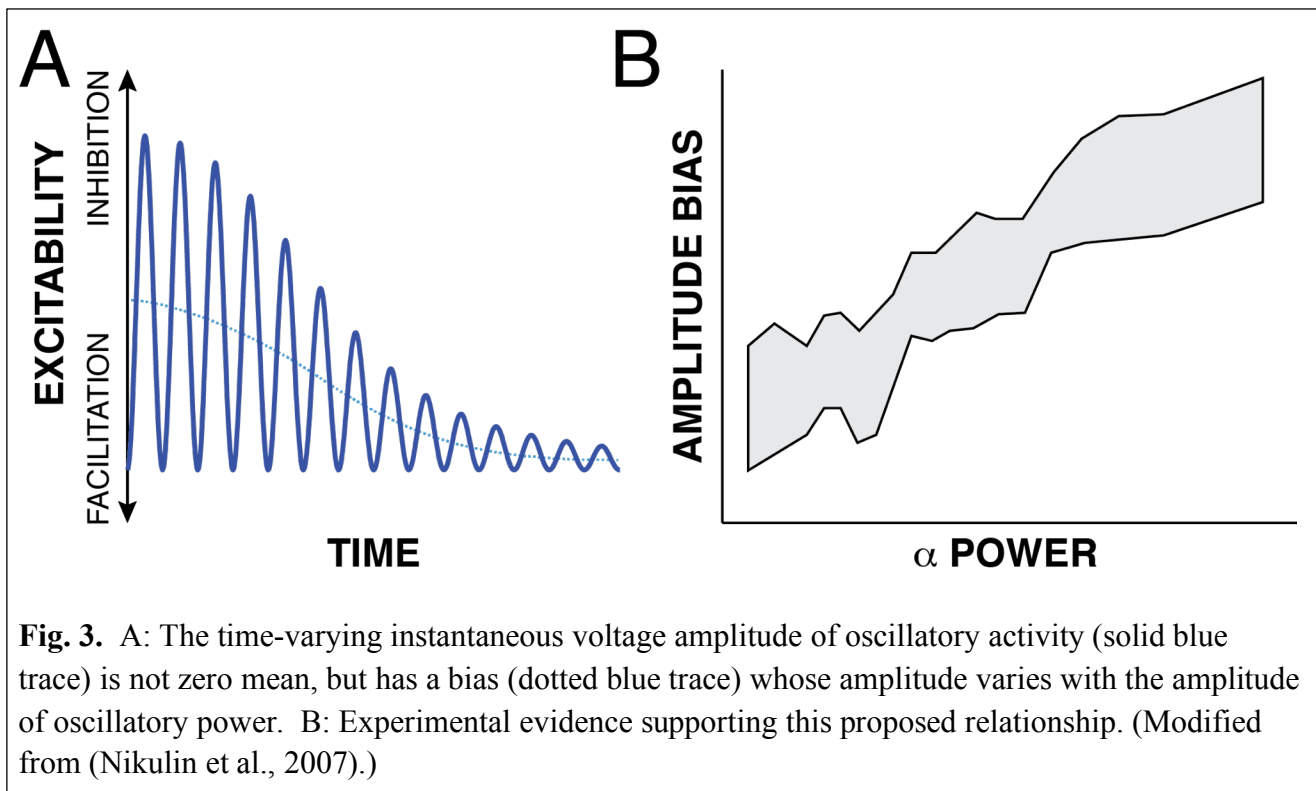


¹ It is important to recognize that the polarity of these voltage changes depends on the recording configuration, and thus may be positive or negative.

171 high level of peak-to-peak amplitude, the concepts of oscillatory voltage amplitude and oscillatory
 172 phase are essentially interchangeable with respect to their relationship to cortical excitability:
 173 excitability is high during a certain phase of the oscillation (i.e., the trough), and excitability is high
 174 when the voltage amplitude is low.

175 It is well known that an oscillation's peak-to-peak amplitude (and hence, oscillatory power) is not
 176 constant but often changes with a task. The next building block supporting the first principle of the
 177 FBO hypothesis is the suggestion that such task-related changes in peak-to-peak amplitude do not
 178 affect the peaks and troughs of the oscillation equally. Let us consider the exemplary oscillatory
 179 signal in Fig. 3-A. In this example, the blue trace gives the time course of oscillatory activity. The
 180 peak-to-peak amplitude of this modulatory signal decreases with time (i.e., reduces oscillatory power
 181 with time), thereby indicating an overall trend toward increased cortical excitability. As recognized
 182 in earlier observations (Mazaheri et al., 2008, Mazaheri et al., 2010, Nikulin et al., 2007) that were
 183 made in the context of explaining evoked responses, such changes in peak-to-peak amplitude might
 184 not affect the amplitude of the peaks and troughs of the oscillatory activity equally, but only affect
 185 the amplitude of the peaks². Indeed, Fig. 3-B (modified from Fig. 3a, Nikulin et al., 2007)
 186 demonstrates that the amplitude bias of an oscillation in the alpha band (y axis) is related to the
 187 power of the oscillation (x axis). (The shaded area gives the 95% confidence interval.) In summary,
 188 the second building block of the first principle of the FBO hypothesis suggests that the amplitude
 189 bias (dotted blue trace, which could be computed by averaging one cycle of the oscillation or by
 190 averaging many trials with random oscillatory phase) is related to oscillatory power.

191 These two building blocks, i.e., instantaneous voltage amplitude of oscillations reflecting cortical
 192 excitability and the existence of a voltage bias, provide the basis for two insights that represent the
 193 main conceptual contribution of the first principle of the FBO hypothesis.



² A later article (Nikulin et al., 2010) came to a somewhat different conclusion.

194 The first insight is that concept of variations in instantaneous voltage amplitude of biased
 195 oscillations provides a simpler, more complete, and more physiologically plausible model of cortical
 196 excitability than a model based on either oscillatory power or oscillatory phase. It is simpler, because
 197 it depends on only one model-free measurement (the instantaneous voltage) rather than on two
 198 separate mathematically extracted transformations (power and phase) that depend on a specific model
 199 (e.g., a repeating sinusoid).

200 This model is also more complete in describing cortical
 201 excitability than a model based on either oscillatory power
 202 or oscillatory phase. This is apparent in the example in Fig.
 203 4. In this example, oscillatory amplitude envelope (dotted
 204 black trace, calculated either by using the Hilbert transform
 205 or by taking the square root of low-pass filtered oscillatory
 206 power) decreases from left to right as the oscillation cycles
 207 between different phases of peaks and troughs. Thus, by
 208 averaging many measurements, a study may well find a
 209 relationship between oscillatory amplitude/power envelope³
 210 and cortical excitability, or between oscillatory phase and
 211 cortical excitability, but neither relationship will be entirely
 212 correct. Specifically, consider the left-most period of the
 213 oscillation in Fig. 4. At time (A), oscillatory power
 214 accurately reflects cortical excitability: power is high and
 215 cortical excitability is low. However, at time (B), there is a
 216 big discrepancy between these measurements as power is
 217 still high but cortical excitability is high as well. In
 218 contrast, for low values of oscillatory power (i.e., around
 219 the times indicated by (C)), oscillatory phase cycles
 220 between the peak and trough (which would suggest
 221 strongly varying cortical excitability), but cortical
 222 excitability is relatively constant and high. In contrast, the
 223 instantaneous voltage amplitude (that includes the voltage bias)
 224 always accurately reflects cortical excitability.

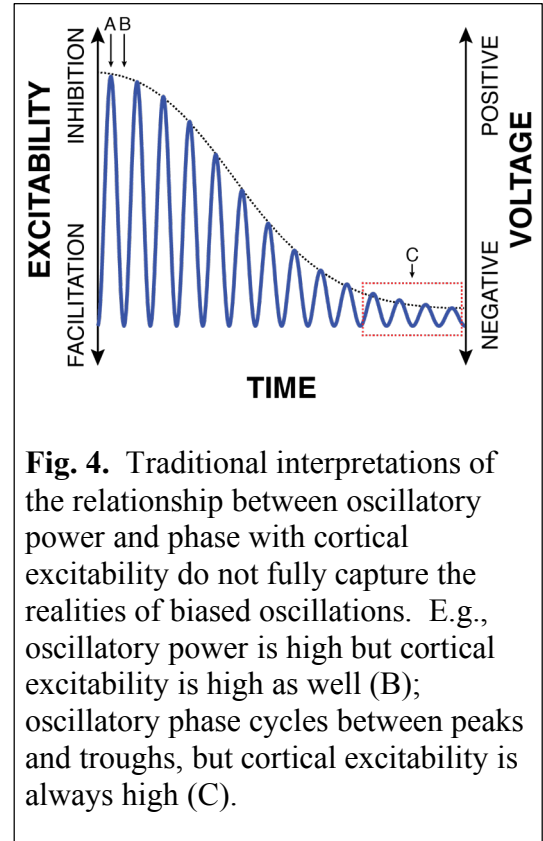


Fig. 4. Traditional interpretations of the relationship between oscillatory power and phase with cortical excitability do not fully capture the realities of biased oscillations. E.g., oscillatory power is high but cortical excitability is high as well (B); oscillatory phase cycles between peaks and troughs, but cortical excitability is always high (C).

225 Finally, this model is also more physiologically plausible. As indicated above, several studies have
 226 found an inhibitory effect of voltage shifts produced by subcortical volleys on firing of cortical
 227 populations (Li, 1956, Li et al., 1956, Tasaki et al., 1954, Von Baumgarten et al., 1952). However,
 228 such physiological interpretations cannot readily be made for the (purely mathematical concepts of)
 229 oscillatory phase or oscillatory power.

230 The presence of the voltage bias also has important implications for the generating principles of a
 231 variety of macroscopic brain signal features. This possibility has been discussed in the specific
 232 context of evoked responses in previous work (Mazaheri et al., 2008, Nikulin et al., 2007). The
 233 second insight is that these implications may be broader than previously discussed. In this context,
 234 let us consider the example given in Fig. 5. The blue trace in panel A illustrates the time course of
 235 the raw (i.e., biased) voltage of an exemplary 10-Hz (i.e., alpha band) modulatory signal in a single
 236 trial. Similar to Fig. 3A, this exemplary modulatory signal reduces the voltage of its peak over about
 237 1.5 seconds, thereby indicating time-varying but still progressively increasing cortical excitability. In

³ The amplitude envelope of an oscillation is the square root of the power envelope. While they are different mathematically, for the purposes of the arguments presented here, they can be used interchangeably.

238 other words, the instantaneous voltage amplitude of this exemplary blue trace is the result of a 10-Hz
 239 oscillation, a slow decrease in peak-to-peak amplitude, and a concomitant decrease in voltage bias.
 240 As will become important later, this slow decrease may suggest the physiologically independent
 241 presence of a very slow oscillation in a frequency analysis.

242 There are several ways to extract oscillatory measurements from brain signals (bandpass-filtering,
 243 Hilbert transform, etc.). The red trace illustrates the result from subjecting the blue trace to a
 244 bandpass filtering operation between 8-12 Hz. Because the bandpass filtering operation removes
 245 frequencies lower than 8 Hz, it removes the oscillation's voltage bias: notice how the voltage bias
 246 (that is readily visible in the blue trace) disappears in the red trace after the bandpass filtering
 247 operation. In other words, the red trace is now centered around zero mean (dashed black line

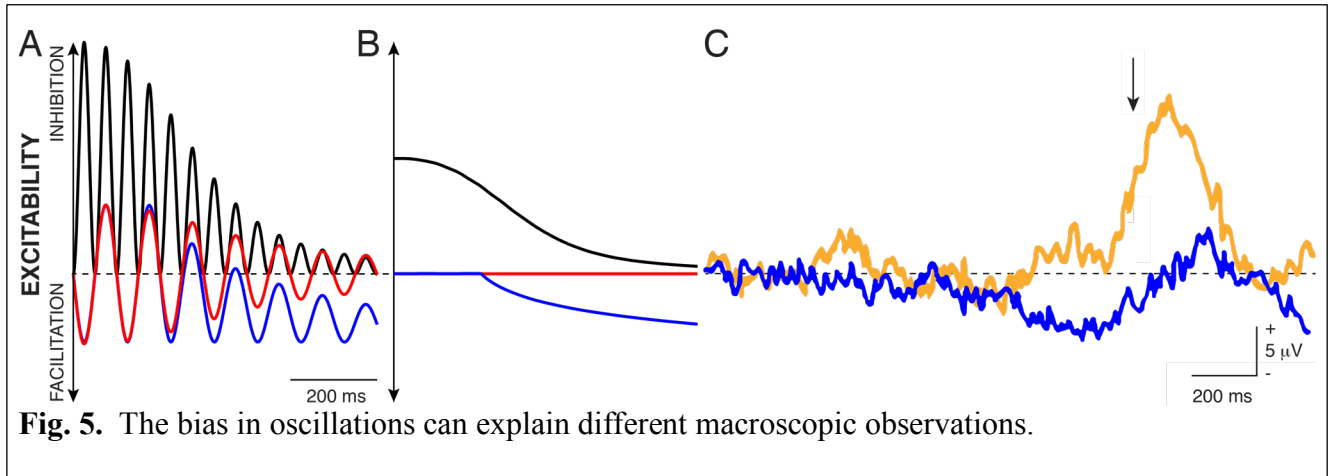


Fig. 5. The bias in oscillations can explain different macroscopic observations.

248 indicating zero voltage). The black solid trace illustrates the instantaneous power (i.e., squared
 249 amplitude) of the bandpass-filtered signal.

250 The blue, red, and black traces in Panel B show the average of many trials of the corresponding
 251 oscillatory signal traces shown in Panel A with random phase. The blue average trace highlights a
 252 trend toward increasing excitability (i.e., decreasing voltage amplitude), similar to what is usually
 253 seen in the Bereitschaftspotential, slow cortical potential, or contingent negative variation. The red
 254 average trace does not show any variations over time. The black average trace highlights the
 255 reductions in oscillatory power typically seen prior to volitional task engagement. Notice the
 256 somewhat smoother appearance of the black trace compared to the blue trace, which results from the
 257 timing uncertainty introduced by the bandpass filtering operation. In summary, the concept of biased
 258 oscillations can explain the relationship between the negative voltage shifts and the decrease in
 259 oscillatory power that are often observed in relationship to particular tasks (such as movements).

260 The literature provides some clues that are consistent with aspects of this hypothesis. One such
 261 piece of evidence is shown in Panel C (modified from Shibasaki et al., 1978). The blue trace
 262 illustrates the average voltage of EEG recordings prior to movement (indicated with an arrow). The
 263 negative deflection prior to movement onset is readily apparent, and is similar to that in the blue trace
 264 in Panel B. The yellow trace illustrates the average voltage of EEG recordings after a lesion to the
 265 nucleus ventralis intermedius (VIM), i.e., the thalamic nucleus that projects to motor cortex. The
 266 yellow trace does not feature the negative deflection prior to movement, but does exhibit an increased
 267 evoked response following the movement. In other words, with an intact VIM, we see the typical
 268 Bereitschaftspotential prior to movement. After the VIM has been lesioned, no such negative voltage
 269 shift occurs, quite possibly because thalamic lesions often diminish alpha oscillations (Hughes et al.,

270 2005). In summary, the second insight of the first principle of the FBO hypothesis is that the
271 amplitude bias in oscillatory activity may explain aspects of the slow time-varying brain signal
272 phenomena that usually precede behaviors.

273 When integrated with other well-known observations, the same concept may also provide a
274 convenient explanation for evoked responses (ERPs) that follow motor movements or sensory
275 stimulation. Specifically, it is well known that the brain can modulate not only the peak-to-peak
276 amplitude but also the instantaneous phase of ongoing low-frequency oscillations. This phenomenon
277 is termed phase resetting and has previously been suggested to be a contributing factor to ERP
278 generation (Fell et al., 2004, Hanslmayr et al., 2007, Makeig et al., 2002, Sauseng et al., 2007, Sayers
279 et al., 1974). However, in addition to phase resetting, it is also well known that different task-related
280 areas in the brain are modulated by different oscillations at similar or different frequencies (Jacobs et
281 al., 2007), and that motor movements or sensory stimulation may result in modulation of oscillatory
282 power (Pfurtscheller et al., 1979, Potes et al., 2014, respectively). All of these known effects will
283 contribute to a time-varying bias in average voltage, and thereby must all provide an important
284 contribution to the generation of ERPs.

285 Finally, biased oscillations may also explain some of the more recent observations reported in the
286 literature, including particular reports of PAC, phase-phase coupling, or amplitude-amplitude
287 coupling (Siegel et al., 2012). As an example, for the representative data shown in Fig. 5A, analyses
288 may identify PAC between the 10-Hz alpha oscillation and the <1 Hz activity change. (See Aru et
289 al., 2014, for a more comprehensive discussion of issues with current analyses or their interpretation.)

290 In summary, the first principle of the FBO hypothesis suggests that the instantaneous voltage
291 amplitude of biased oscillations is the principal measurement that controls cortical excitability, and
292 that it can help to explain a variety of macroscopic brain signal phenomena.

293

294

295 **2.2. The Second Principle: A General Framework for Dynamic Cortical Function**

296 The second principle synthesizes and extends the concepts provided in the CTC hypothesis and the
 297 gating-by-inhibition framework by embedding the concept of biased oscillations into a predictive
 298 context. The result provides a simple and general model for routing of information flow that can
 299 explain dynamic cortical function.

300 Similar to the proposal that biased oscillatory voltage amplitude provide a unifying foundation for
 301 explaining experimental results for oscillatory power and phase, control of local cortical excitability
 302 with biased oscillations can also provide a unifying foundation for synthesizing CTC and gating-by-
 303 inhibition. The proposal is that rather than controlling the phase relationship of oscillations across
 304 task-related populations (as proposed by CTC) or oscillatory power of neuronal populations (as
 305 proposed by gating-by-inhibition), the brain engages in dynamic task-related processing by
 306 controlling the instantaneous voltage amplitude of biased oscillations to predictively inhibit task-
 307 unrelated populations or inhibit populations at task-unrelated times.

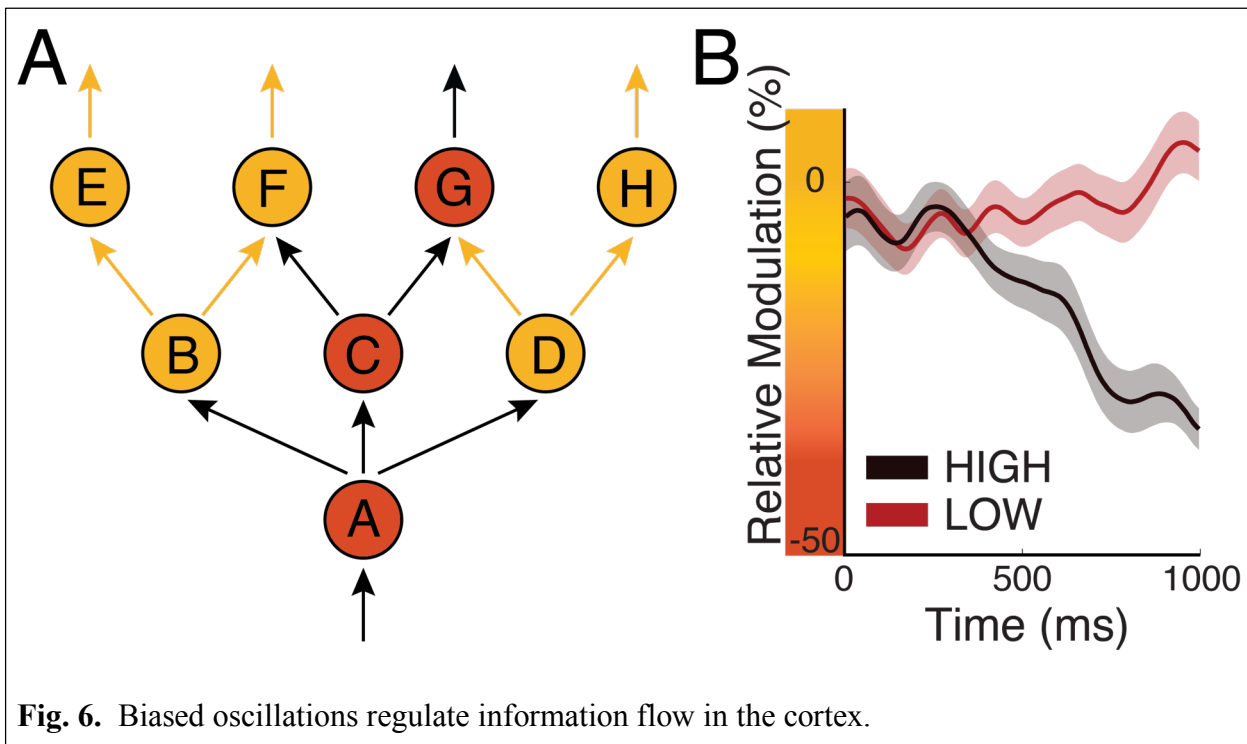


Fig. 6. Biased oscillations regulate information flow in the cortex.

308 To illustrate this concept, let us consider the exemplary network of neuronal populations that is
 309 shown in Fig. 6-A. In this figure, eight distinct neuronal populations are labeled with A-H.
 310 Anatomical connections between these populations are depicted with arrows. Arrows that do or do
 311 not carry action potential volleys are shown in black or yellow, respectively. Populations that receive
 312 excitatory or inhibitory modulation (i.e., low or high average peak-to-peak voltage amplitude,
 313 respectively) are shown in orange or yellow, respectively. In this example, population A, which does
 314 not receive inhibitory modulation (e.g., from subcortical structures such as a particular thalamic
 315 nucleus), receives an action potential volley and sends out volleys to all populations it is connected to
 316 (B, C, and D), presumably through cortico-cortical projections. Because B and D receive inhibitory
 317 modulation, they are not excited by the incoming volleys they receive from A; thus, they do not send
 318 out volleys to connected populations. In this example, excitatory input to population A will result in

319 activation of, and communication between, populations C and G. This concept synthesizes the CTC
320 and gating-by-inhibition hypotheses: because biased oscillatory voltage amplitude can define higher
321 excitability either by decreasing peak-to-peak amplitude or by being in its trough, it can describe a
322 situation in which a sending and a receiving neuronal population communicate either by
323 synchronizing their phases (as would be suggested by CTC) or by decreasing the peak-to-peak
324 amplitude of the receiving population (as would be suggested by gating-by-inhibition).

325 The second principle anchors the dynamics of biased oscillations in a predictive process.
326 Dynamic information routing may require separate mechanisms for task-related engagement that can
327 or cannot be predicted based on prior evidence. There are obvious situations in which our
328 interactions with our environment can be predicted in advance. For example, we may be provided
329 with accumulating perceptual evidence that will lead to a motor action. In this situation, the brain
330 has the opportunity to optimize excitability of its neuronal populations (e.g., increase excitability of
331 the motor system) so as to optimize performance. Indeed, many studies (Bertelson et al., 1960) have
332 documented increased behavioral performance resulting from prior evidence. According to the first
333 principle of the FBO hypothesis, the brain may readily achieve this purpose by reducing the peak-to-
334 peak amplitude of biased oscillations associated with neuronal populations that are related to the
335 anticipated task, and by increasing it for all other populations. There is plenty of experimental
336 evidence to support this concept (e.g., Bidet-Caulet et al., 2012). Fig. 6-B (modified from Kubanek
337 et al., 2013) illustrates the relative power (i.e., a function of peak-to-peak amplitude) of an oscillatory
338 signal recorded over sensorimotor cortex in a perceptual decision task, in which subjects were asked
339 to push a button depending on the amount of evidence given by auditory clicks. The power of the
340 modulatory signal is progressively reduced for trials of “high” evidence compared to for trials of
341 “low” perceptual evidence. Thus, this mechanism progressively increases cortical excitability in
342 motor cortex, and clearly demonstrates that cortical excitability of local neuronal populations
343 depends not only on present but also on past events.

344 It is important to recognize that this optimization of brain function cannot readily be achieved by
345 generating a desired phase relationship between neuronal populations: in the predominant situation
346 in which the timing of task execution is not precisely predictable (e.g., in the example above, it is not
347 exactly clear when the movement will occur), a desired functional relationship between two cortical
348 populations can only be achieved using phase synchrony if oscillations governing two different
349 neuronal populations share the same frequency. This is plausible for populations within a particular
350 cortical system (e.g., the visual system), which may be subserved by the same subcortical nucleus.
351 Indeed, existing experimental evidence for such phase synchrony across populations (Roberts et al.,
352 2013, Saalman et al., 2012) was derived from data collected within the visual system. At the same
353 time, it is well known that oscillations in different systems can be produced by different sources, and
354 often have different frequencies (Pineda, 2005). E.g., the frequency of the sensorimotor mu rhythm
355 has been reported to be significantly higher than that of the classical visual alpha rhythm (Storm van
356 Leeuwen et al., 1976). Thus, if the timing of task execution is not known ahead of time, it appears to
357 be difficult if not impossible for the brain to predictively control information flow by achieving
358 constant phase synchrony across such different systems. This suggests that CTC cannot explain the
359 regulation of information flow across wide areas of the brain in such situations.

360 The situation is opposite if the brain has to process and react to a stimulus that cannot be
361 anticipated, e.g., a loud noise while we are reading. While it is well known that we can quickly react
362 to such unexpected stimuli (Yantis et al., 1984), such rapid reactions cannot readily be explained by
363 increased excitability that are due to reduction in oscillatory peak-to-peak amplitude, as highest
364 excitability would not be achieved until the oscillation reaches its trough (i.e., up to tens of ms later).

365 Thus, reducing the peak-to-peak amplitude of a biased oscillation would not guarantee that the initial
366 action potential volleys produced by the stimulus would hit excitable neuronal populations in the
367 appropriate sensory regions, and consequently would reduce the ability of the brain to process this
368 stimulus. At the same time, it is well known that the brain has the ability to reset the phase of
369 oscillatory activity (Brandt, 1997) in response to salient stimuli. With phase-resetting of biased
370 oscillations, the brain could produce oscillatory phase synchrony throughout the respective
371 perceptual system. Thus, it would guarantee that action potential volleys produced by such stimuli
372 would be delivered to excitable neuronal populations throughout that system. While there is
373 evidence for cross-modal phase resetting (Thorne et al., 2011), the degree to which different systems
374 are phase reset by an incoming stimulus may be a critical determinant of the limitations of human
375 performance in sensori-motor behavior. Such phase resetting may even cause subsequent reduction
376 in peak-to-peak amplitude in this perceptual system. Hence, in response to a sudden salient stimulus,
377 the brain may update its ongoing predictions to incorporate the likely case that more salient stimuli
378 will follow the first.

379 Irrespective of whether an event can or cannot be predicted based on prior evidence, such
380 configurations fundamentally requires the brain to make predictions: in the decision-making
381 example above, the brain must use current and past evidence to make a prediction of the optimal
382 future state of cortical excitability. In the example of a loud noise during reading, the brain must be
383 able to evaluate the likelihood that a particular stimulus occurs given past evidence (e.g., we know
384 that a loud stimulus in a library will produce a stronger cortical response than a loud stimulus in a
385 predictive series of loud stimuli). In other words, the brain must constantly use information from
386 past events to predict the likelihood of a particular stimulus, and adjust cortical excitability as a
387 function of this predicted likelihood. This invokes an image in which the “excitability landscape”
388 across the cortex serves to is constantly being updated using a predictive process.

389 In summary, the second principle of the FBO hypothesis suggests that variable cortical function is
390 implemented primarily by variable biased oscillations across different cortical populations, and
391 proposes that the variability of the two main parameters of biased oscillations, i.e., oscillatory peak-
392 to-peak amplitude and phase, must be determined by a predictive process. Thus, predictive biased
393 oscillations can form the basis for a simple, general, and physiologically grounded model of variable
394 cortical function.

395 **3. Predictions**

396 The FBO hypothesis generates a number of testable predictions. The first principle of the FBO
397 hypothesis predicts: 1) that for most if not all locations in the cortex that are modulated by
398 oscillatory activity, oscillatory activity has a voltage bias that is related to oscillatory power; 2) that
399 the instantaneous voltage of biased oscillations is a better predictor of cortical excitability (e.g., as
400 assessed by action potential firing probability or by the magnitude of broadband gamma amplitude⁴)
401 than is oscillatory power or phase; 3) that amplitude variations in biased oscillatory signals can
402 explain a fraction of the variance of slow time-domain signals (such as the BP), of evoked responses,
403 and of more recent observations (in particular amplitude-amplitude coupling or PAC that involves
404 frequencies < 4 Hz); and 4) common evoked responses (ERPs) that are routinely detected in
405 EEG/MEG may not be detectable in LFP or ECoG signals, because ERPs represent at least in part the

⁴ Broadband gamma amplitude is often computed by determining the analytic amplitude of ECoG/LFP signals in a high (e.g., 70-170 Hz) frequency band. Broadband gamma activity has been suggested by an increasing number of studies to reflect the average firing rate of neuronal populations close to the electrode (Manning et al., 2009, Miller et al., 2009, Ray et al., 2011).

406 spatially superimposed time-domain voltage changes associated with a temporal sequence of
407 oscillatory power adjustments that are the consequence of a stimulus.

408 The second principle of the FBO predicts: 1) that variable routing of information flow through a
409 physical network depends primarily on the cortical excitability (indexed by biased oscillations) of the
410 receiving neuronal population; 2) that the peak-to-peak amplitude of a biased oscillation is produced
411 by a prediction of the likelihood that the corresponding neuronal population is related to the task; 3)
412 that the phase of a cortical oscillation is adjusted as a function of a prediction of the likelihood of a
413 sensory stimulus; 4) that differential oscillatory activity should be present not only across different
414 systems (e.g., visual vs. motor), but also within a particular system; and 5) that task execution (rather
415 than predictive network modulation) should always be accompanied by non-oscillatory broadband
416 gamma activity.

417 Testing these predictions requires careful consideration of several technical issues. First, any
418 particular cortical population may be under simultaneous and superimposing modulatory influence
419 by different oscillations (e.g., Hughes et al., 2007, Jacobs et al., 2007). Second, the raw voltage
420 potential may be influenced by non-oscillatory activity (e.g., voltage shifts created by ionic currents).
421 Third, voltage is not an absolute but a relative measurement. Thus, an experimentally measured
422 voltage bias may be of varying magnitude or even polarity depending on sensor modality and source
423 of referencing. Fourth, with present signal acquisition hardware, it is difficult to achieve similar
424 signal-to-noise characteristics across all relevant signal frequencies (i.e., DC to high gamma). Fifth,
425 oscillatory modulation is likely to be spatially fine-grained, and hence may be subjected to spatial
426 summation, which will impede its proper characterization using EEG or MEG. Thus, testing these
427 predictions may benefit greatly from, and will likely require, intracranial or intracortical recordings.

428 4. Further research

429 The FBO hypothesis provides a proposal for two general mechanisms that can support dynamic
430 cortical function. Its main predictions listed above can now readily be tested in future experimental
431 research. In addition, there are several important questions that remain to be answered.

- 432 1. In line with previous findings, this paper suggests that there is an asymmetric distribution of peak
433 and trough amplitudes. The specific characteristics of this asymmetry are currently unclear.
- 434 2. Is cortical excitability influenced by factors other than instantaneous voltage?
- 435 3. Other than instantaneous cortical excitability, which factors (such as amplitude or temporal
436 distribution) of input to a given region determine cortical excitation?
- 437 4. Why is cortical excitability established using repetitively pulsed inhibition (i.e., oscillatory
438 activity) rather than using a continuous process? I speculate that repetitive inhibition may be
439 more metabolically efficient than continuous inhibition, and may be equally effective.
- 440 5. The second principle of the FBO hypothesis explains how the brain may predictively modulate
441 cortical function. It does not attempt to answer several important corresponding questions:
 - 442 a. How does the brain generate predictive models of optimal cortical excitability?
 - 443 b. How does the brain use sensory inputs resulting from particular behaviors to change the
444 parameters of these predictive models to optimize future behaviors?
 - 445 c. The predictive processes described in the FBO hypothesis essentially bias cortical
446 processing towards those neural populations that are task-related. It does not elucidate the
447 nature of the cortical activations that actually execute the tasks (i.e., primarily detected
448 using action potential firing rates or broadband gamma amplitude). The relationship
449 between these two processes is important, because they lead to different predictions about

450 measurements. As an example, according to the FBO hypothesis, presentation of multiple
451 sensory stimuli will lead to an increase in cortical excitability in the regions
452 corresponding to the particular sensory domain. Thus, subsequent stimuli should result in
453 augmented cortical responses. However, many experiments have shown that repeated
454 stimulation can result in decreased responses, a phenomenon called repetition suppression
455 (Baldeweg, 2006). This phenomenon may be explained by the concept of *predictive*
456 *coding* (Clark, 2013, Friston, 2010), which postulates that coding of information in the
457 brain at least in part represents the discrepancy between a prediction of a sensory stimulus
458 and the actual stimulus. In summary, these two concepts may lead to completely opposite
459 experimental results. Future research is necessary to establish the interplay between these
460 two phenomena.

461

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467 **6. References**

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